Section A-Research paper



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# Abstract

Cancer constitutes a large group of diseases and is a prime cause of death worldwide. Erhlich ascites carcinoma (EAC), an extemporaneous murine adenocarcinoma, is one of the wellrecognized models in cancer research. Diosgenin (DGN) is a naturally occurring steroidal saponin from fenugreek and wild yam. Polymer nanoparticles have potential applications in biomedicine, but one of the important concerns is their safety. The present study aimed to evaluate the anti-cancer activity of diosgenin-encapsulated PLGA nanoparticles (PLGA-DGN NPs) against Ehrlich ascites carcinoma. The synthesized PLGA-DGN NPs were characterized by dynamic light scattering and surface zeta potential measurement, UV-vis spectroscopy, and Fourier transform infrared (FTIR) spectroscopy. The antineoplastic potency of PLGA-DGN NPs against EAC cells was assessed through cell viability assay, oxidative stress, chromatin condensation, and cell cycle arrest by flow cytometry. The cytotoxicity of PLGA-DGN NPs in EAC cells indicates the MTT assay revealed that high cytotoxic efficacy of PLGA-DGN NPs against EAC cells with the IC<sub>50</sub> value of PLGA-DGN NPs was 7.91µg/ml. The oxidized glutathione (GSSG) increased compared to EAC control and decreased the level of reduced glutathione (GSH) in PLGA-DGN NPs, DGN rather than EAC control. In EAC cells, ROS formation was determined by H2DCF2DA staining using fluorescence microscopy showed PLGA-DGN NPs elevated the intracellular ROS generation at their respective IC<sub>50</sub> doses

Section A-Research paper

indicating potent apoptotic activity compared to DGN-treated EAC cells and EAC control. PLGA-DGN NPs exhibited cytotoxicity and induced apoptosis by increasing reactive oxygen species, chromatin condensation, cell cycle arrest at the G2/M phase, expression of pro-apoptotic proteins, and mitochondrial dysfunction in EAC. All the results indicate that PLGA-DGN NPs exert cytotoxic, oxidative stress, and apoptotic effect. In conclusion, the findings demonstrate that PLGA-DGN NPs may act as potential beneficial agents in carcinoma chemoprevention. **Keywords**: Diosgenin, PLGA; EAC; Oxidative stress; Cell cycle arrest.

# Introduction

One of the most common experimental tumors, Ehrlich ascites carcinoma (EAC), is crucial for modeling. It was used as an experimental tumor by Ehrlich and Apolant, in 1905[1], when it initially appeared as spontaneous breast cancer in a female mouse[2]. Tumour tissues were transplanted under the skin from one mouse to another. EAC, an undifferentiated carcinoma, is initially hyperdiploid, highly transplantable, non-regressive, rapidly increasing, brief in life span, and 100% malignant. According to a recent study, cisplatin co-treatment against Ehrlich ascites carcinoma resulted in substantial reductions in tumor cell number, viability, growth rate, and proliferative potential, as well as enhanced apoptosis and G0/G1 and sub-G1 cells cycle arrest[3]. The effectiveness of *in vivo* anti-proliferative therapy against EAC cells was also examined. Genestin showed a significant reduction in tumor weight, volume, high-mobility group box 1 (HMGB1), and nuclear factor-kappa B (NF-B) levels as compared to the control group[4]. The cancer chemotherapeutic strategies need to shift from discovery to novel cancer therapies to refining existing strategies and diagnostics in effective, advanced, and plausible ways[5].

Nanotechnology may be a possible solution by implementing it in cancer management. Nanotechnology offers novel therapeutic strategies with better targeting specificity, increased drug localization with high efficiency, reduced systemic toxicity, better improvement of diagnostic specificity, and improved imaging and radiation therapy[5]. The nanoparticles made by advanced nanotechnology is a promising contender in controlled drug delivery system (DDS)[6]. Nanocarrier-mediated drug delivery has been exploited to circumvent rapid degradation, low bioavailability, and inactivation of chemotherapeutic drugs[7]. In cancer nanotherapeutics, the application of polymeric nanoparticles (PNP) is gaining attraction due to its higher drug delivery efficiency, improved drug solubility, good pharmacokinetic profile, prolonged blood circulation time, and negligible side effects[8]. Polylactide-co-glycolide (PLGA) is an FDA-approved polymeric nanoparticle widely used for drug delivery for its biocompatibility, biodegradability, and non-toxic profile[9]. With the advent of nanomedicine, PLGA as a nanocarrier has found applications in various fields of medical research, such as biomechanics, chemotherapy, and immunology.

Phytochemicals, non-nutritive plant compounds with disease-protective or -preventive qualities, have been the subject of numerous investigations[10]. These substances are non-essential nutrients, meaning the human body does not need them to maintain life. Approximately 80% of

#### Section A-Research paper

all breast cancer cases are ER (+). Tamoxifen and aromatase inhibitors are two examples of hormone treatments now used to treat ER (+) breast cancer[11]. Diosgenin (DGN) is a phytosterol saponin, mainly found in many plant species, including Trigonella foenum-graecum (fenugreek), Heterosmilax species, and Dioscorea species, particularly the roots of wild yam (Dioscorea villosa) [12]. About 137 types of Dioscorea species are considered the primary source of DGN; among them, 41 species contain more than 1% DGN[13]. A study by [14], proposed that DGN significantly inhibited the MCF-7 cell's proliferation by modulation of methylation status and microRNA-145 activation, but the migration capacity of MCF-7 cells was inhibited with a higher dose of DGN. Diosgenin was found to be a sensitive anti-cancer agent for triple-negative breast cancer cell line HCC1937 [15]. Inhibition of cell proliferation was observed in a dose and time-dependent manner after the treatment with DGN. Besides that, DGN induced apoptosis through the Bcl-2 associated X protein (Bax), caspase3 protein. Dioscin, an analog of DGN, induced apoptosis-mediated cell death by inhibiting pro-apoptotic proteins and inhibiting the invasion property of breast cancer cells by enhancing the GATA-binding protein 3 (GATA3)[16]. However, DGN is deprived of its clinical application due to its high hydrophobicity, poor bioavailability, and side effects.

Presents study aimed to synthesize non-toxic, biodegradable diosgenin-encapsulated PLGA nanoparticles (PLGA-DGN NPs) and evaluate it's *in vitro* anti-cancer potential against EAC cells.

## Experimental

**Materials and methods:** Diosgenin ( $\geq$ 93%), Poly (D, L-lactic-co-glycolic) acid (PLGA) (lactic acid: glycolic acid 50:50) (Mw = 18,000), Dimethyl sulfoxide (DMSO), 3-(4,5-dimethyl-2-thiazolyl)-2,5-diphenyl-tetrazolium bromide (MTT), and F-68 (Poloxamer 188), penicillin and streptomycin were purchased from Sigma Aldrich Co, LLC, US. Propidium iodide, DAPI, and Fetal bovine serum (FBS) were procured from GIBCO. Merck provided all the chemicals and reagents used in the current investigation, which were all analytical quality.

#### Preparation of DGN-encapsulated PLGA nanoparticles

Diosgenin-encapsulated PLGA Nanoparticles (PLGA-DGN NPs) were formulated by the Nano precipitation technique described in our previous publication[9] with minor modifications. In brief, a weight amount of PLGA and DGN were co-dissolved in organic solvent acetone and vortexed for completely dissolved. Then an aqueous phage was prepared by taking 20 ml millipore water containing Pluronic F-68 solution (0.5%, w/v). Drop by drop, the organic phase was introduced to the aqueous phase while being stirred moderately magnetically overnight at room temperature. Acetone was completely evaporated, and the nanosuspension (MWCO: 12kDa) was then purified through dialysis. Then purified nanosuspension was centrifuged at 20,000 rpm at 4°C for 30 minutes, and the pellet was washed with PBS (pH 7.4) and, finally, lyophilized to obtain freeze-dried PLGA-DGN NPs. The entrapment efficiency (EE%) and loading capacity (LC%) were analyzed according to our previously reported methods[9].

Section A-Research paper

#### Characterization

Dynamic light scattering (DLS) and electrophoretic light scattering (Laser Doppler, Malvern Instruments, U.K.) techniques were used to assess the size of PLGA-DGN NPs at 25°C at a 90° angle[17]. Zeta-sizer Nano ZS (ZEN 3600, Malvern Instruments, U.K.) was used to elaborate on the zeta potential measurements on the instrument equipped with a combination of Laser Doppler Velocimetry at 25°C. To assess the broadness of molecular weight distribution, The polydispersity index (PDI) PDI index is usually measured, and a larger PDI indicates broader molecular weight. The pH was fixed during the measurement in all samples. The entrapment efficiency (EE%) and loading capacity (LC%) were 78.68% and 8.38% respectively.

A UV-VIS-NIR spectrophotometer (UV-VIS-NIR spectrophotometer-3600, Shimadzu) was used to measure the PLGA-DGN NPs' absorption spectra. A 200-400 nm wavelength range was used to measure the absorbance spectra of DGN, VPLGA NPs, and PLGA-DGN NPs.

Fourier transforms infrared spectroscopy (FTIR) study of PLGA-DGN was carried out using an FTIR spectrophotometer (Perkin Elmer Spectrum Express Version 1.03.00), and the spectrum was recorded in the range of 4000–400 cm<sup>-1</sup> with an accuracy of  $\pm 0.01$  cm<sup>-1</sup> and resolution of 4 cm<sup>-1</sup>. Samples were mixed with potassium bromide (KBr) and compressed using a pressure of 200 kg/cm<sup>2</sup> for 2 min in a hydraulic press to make the pellets. FTIR spectra were observed using an FTIR spectroscope at the wavelength of 4000 to 400 cm<sup>-1</sup> [9].

## Cell culture and maintenance

The murine Ehrlich ascites carcinoma (EAC) cells were purchased from Chittaranjan National Cancer Institute, Kolkata, India. Cells were grown in a DMEM medium (GIBCO BRL, USA) containing 10% FBS (GIBCO BRL, USA) and antibiotics in appropriate conditions. Cell lines were cultured and maintained in Dulbecco's modified Eagle's medium (DMEM), supplemented with 10% fetal bovine serum (FBS), 2 mM L-glutamine, penicillin (100 units/mL) and streptomycin (100  $\mu$ g/mL) under humidified atmosphere (95%) and 5% CO<sub>2</sub> at 37°C in a Co<sub>2</sub> incubator.

## Anti-cancer activity

## Cytotoxicity assay (MTT test)

A cell viability study was performed against EAC cells by 3-(4,5-dimethyl-2-thiazolyl)-2,5diphenyl-tetrazolium bromide (MTT) assay[9]. Cells were seeded separately in 96-well plates at  $1 \times 106$  cells/well density and grown for 72 hours. After cells reached 80% confluence, they were treated with different concentrations of free DGN and PLGA-DGN and incubated for 72 hours in a CO<sub>2</sub> incubator. To assess time-dependent cell viability, we assessed cell viability at different time points (24, 48, and 72 hours). At this predetermined time interval, freshly prepared MTT solution (5 mg\/mL) was added to each well, and the plate was incubated at 37°C for an additional 4 hours. During this incubation, formazan crystals formed and were solubilized by adding DMSO (0.1%) and mixed well by shaking the plate for 10 seconds. Absorbance was then measured at 540 nm using an ELISA analyzer (Bio-Rad, model 680). Experiments were performed in triplicate, and results are presented as mean  $\pm$  SD standard deviation.

Section A-Research paper

# **Study of Oxidative Stress**

## Measurement of Intracellular ROS generation

EAC cells were treated with DGN and PLGA-DGN NPs for 24 h at their respective  $IC_{50}$  doses. The next day, cells were washed with phosphate buffer, incubated with 1 µg/mL H<sub>2</sub>DCFDA for 30 min at 37°C, and rewashed thrice with culture media. Cells were found using a fluorescent microscope (LEICA DFC295 from Germany) and a fluorescence spectrophotometer (Hitachi F-7000) at 485 nm excitation and 520 nm emission, respectively. The experiment was done three times[17].

Measurement of reduced glutathione (GSH) and oxidized glutathione (GSSG)

Intracellular GSH AND GSSG were estimated by EAC cells with free DGN and PLGA-DGN NPs for 24 h at their respective  $IC_{50}$  doses. The next day, culture media was removed, and performed cell lysis by lysis buffer (0.1% Triton, 5 mM EDTA, 1 mM PMSF). The cell lysate was extracted, and sulfosalicylic acid (4%) was mixed with it, followed by centrifugation. Finally, GSH concentration was measured by DTNB assay[17]. To calculate the GSSG concentration, 2  $\mu$ L of 2-vinyl pyridine was mixed with the samples and then performed DTNB assay.

## Lactate dehydrogenase (LDH) release assay

EAC cells  $(1 \times 10^{6} \text{ cells/well})$  were treated with DGN and PLGA-DGN NPs for 24 h at their respective IC<sub>50</sub> doses. The next day, culture media was removed, and a reaction mixture containing pyruvic acid, triton X-100, in PBS buffer (pH 7.4). Then 100 µL of reduced NADH (0.4 mg/mL) was added to the sample, and finally, the absorbance was taken at 340 nm by an ELISA microplate reader (Bio-Rad, Model 680)[18].

## Study of chromatin condensation

Chromatin condensation was observed by DAPI and propidium iodide (PI) staining[17]. In brief, EAC cells ( $1 \times 10^6$  cells/well) were exposed to DGN and PLGA-DGN NPs for 24 hours at their corresponding IC50 concentrations. Cells that have not been treated are regarded as the control group. Then cells were washed with PBS (pH 7.4), 4% paraformaldehyde solution was used for cell fixation and then stained by DAPI (0.5 g/mL) and RNAse-PI (1mg ml<sup>-1</sup>) for 15 min at 37°C. Finally, cells were washed twice with PBS, and images were taken by a fluorescence microscope (LEICA DFC295, Germany).

# Cell cycle study

EAC cells ( $1 \times 10^{6}$  cells) were treated with DGN and PLGA-DGN at their respective IC<sub>50</sub> doses for 24 h. After that, cells were washed thrice by centrifugation at 2000 rpm for 5 min, followed by fixation using 70% chilled ethanol. Then cells were again centrifuged for washing and treated with RNAse A (10 µL) at 37°C for 1 h. Then propidium iodide (25 µL) staining was performed in the dark at room temperature. After washing with PBS (pH 7.4), DNA content in the cell was analyzed by a flow cytometer (BD FACSVerse)[19].

## **Statistical analysis**

All results were presented as mean  $\pm$  standard deviation (S.D.) for all studies carried out in triplicate. One and two-way analysis of variance (ANOVA) was used to analyze the data's

Section A-Research paper

statistical significance and multigroup comparisons. Then GraphPad Prism and Origins 8 (OriginLab, Northampton, USA) were used for the Tukey post hoc test. All Statistical significance was considered at p < 0.05.

# **Results and Discussion**

The hydrodynamic diameters and size distribution of PLGA-DGN NPs were investigated utilizing the DLS technique. Results showed particle size 147.98  $\pm$  3.45, and the size distributions were mono-dispersed. The  $\zeta$ -Potential of the PLGA-DGN NPs exhibited negative values of 26 mV $\pm$ 0.62 (Table 1).

The UV-Vis and FTIR spectroscopic analysis was discussed in our previous paper (Dey et al., 2022). The report exposed that DGN showed a maximum absorbance peak at  $\lambda_{max}$ =210 nm, which was shifted to  $\lambda_{max}$ =213 nm after forming PLGA-DGN NPs. An increment of the polarity of PLGA-DGN NPs might cause this shifting.

FTIR spectra showed (Figure 1F) the characteristic bands of DGN at 3457 cm<sup>-1</sup>, 2948 cm<sup>-1</sup>, 2800-and 3600 cm<sup>-1</sup>, respectively, due to -OH, -CH<sub>2</sub>, -CH<sub>3</sub> stretching vibration. PLGA-DGN NPs exhibited all these characteristic peaks at 3642 cm<sup>-1</sup>, 3490 cm<sup>-1</sup>, 2941 cm<sup>-1</sup>, and 1759 cm<sup>-1</sup>. Though some minor peaks shifting was noted due to hydrogen bonding, van der Waals' force, and dipole-dipole interaction[9].

**Table 1.** Characterization of PLGA-DGN NPs. Result is expressed as (mean  $\pm$  S.D.; n = 3).

Formulation	Hydrodynamic Size (nm)	polydispersity index (PDI	Zeta potential (mV)	entrapment efficiency (EE%)	Loading capacity (LC%)
PLGA-DGN NPs	147.98±3.45	0.125±0.02	-28±0.52	78.68±6.13	8.38±1.84

# Cytotoxic effect of PLGA-DGN NPs against EAC cells

Cell viability was examined in a concentration and time-dependent manner using the MTT assay. The results showed that PLGA-DGN NPs significantly inhibited EAC cell viability with increasing concentrations compared to DGN (Fig 1). The IC<sub>50</sub> values were 7.91  $\mu$ g/mL for DGN and 1.62  $\mu$ g/mL for PLGA-DGN-NP. PLGA-DGN NPs also showed a significant decrease in cell viability at 48 and 72 hours, respectively. Cell viability studies revealed that PLGA-DGN NPs have significant cytotoxic potential compared to DGN[9].

Section A-Research paper



**Fig 1.** *In vitro* cell viability study in EAC cells after the treatment with DGN and PLGA-DGN NPs against at different concentrations (0.001 to 100  $\mu$ g/mL) Results are expressed as (mean ± S.D; n=3; \*p<0.05, \*\*p<0.01, \*\*\*p<0.001)

## **Evaluation of oxidative stress**

The potential of PLGA-DGN NPs to produce oxidative stress in EAC cells was evaluated by measuring free radicals and antioxidant activity. Results showed that after the treatment with PLGA-DGN NPs, the DCF intensity was significantly increased compared to free DGN. This DCF was formed from non-fluorescence H<sub>2</sub>DCFDA by oxidation reaction in the presence of ROS and has given bright green fluorescence (Fig 2 & Fig 3). Besides that, PLGA-DGN NPs also induced the GSH to GSSG conversion. As shown in Fig 3, the GSH levels decreased significantly, and the GSSG level was increased in the PLGA-DGN NPs treated group compared to DGN. A significant increase in LDH level in EAC cells was also observed in PLGA-DGN NPs treated group compared to free DGN (Fig 3). Hence, these results confirmed that PLGA-DGN NPs produced oxidative stress in EAC cells by generating excessive ROS.

## **Study of nuclear morphology**

Nuclear morphology was analyzed by evaluating chromatin condensation in EAC cells. Cells were stained with DAPI and PI to study chromatin condensation. Fig 2 presented shrunken and irregular nuclear morphology with red spherical beads in DAPI and PI-stained cells in the PLGA-DGN NPs treated group. However, no notable change was visualized in DGN-treated groups.

Section A-Research paper



**Fig 2.** Study of ROS generation and chromatin condensation in EAC cells after the treatment with DGN, PLGA-DGN NPs. Fluorescence microscopic observation of intracellular ROS generation by H2DCFDA staining, nuclear morphology by DAPI, and PI staining. Scale bar: 50  $\mu$ m



Fig 3. Measurement of DCF fluorescence intensity in ROS generation by spectrofluorometer; Measurement of reduced glutathione (GSH), oxidized glutathione (GSSG) and Lactate dehydrogenase (LDH). Results are expressed as (mean  $\pm$  S.D; n=3; \*p<0.05, \*\*p<0.01, \*\*\*p<0.001)

## **Evaluation of cell cycle arrest**

The proportion of the cell population in the G2/M phage of the cell cycle was considerably higher in the PLGA-DGN NPs treated group, according to the flow cytometry analysis of the cell cycle. Whereas no significant cell cycle change was observed in the DGN-treated group. So, PLGA-DGN NPs induced cell cycle arrest at the G2/M phage (Fig 4).



**Fig 4.** Flow cytometry analysis of cell cycle. Figure shows the percentage of cells at different pages of the cell cycle (A-B).

# Conclusion

In this investigation, we successfully prepared and characterized biodegradable, biocompatible, and non-toxic PLGA-DGN NPs with desirable sizes with narrow distribution and high loading capacity. We epitomized the hypothesis that PLGA-DGN NPs stimulate ROS generation and produce oxidative stress, which induces chromatin condensation. Simultaneously, PLGA-DGN NPs induced cell cycle arrest at G2/M phage, exerting a cytotoxic effect through oxidative stress-mediated cell death.

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## **Disclosure statement**

All authors declare that they have no conflict of interest.

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Section A-Research paper

## Abbreviation

EAC-Ehrlich ascites carcinoma cells DGN-Diosgenin PLGA- Poly (D, L-lactic-co-glycolic) acid PLGA-DGN NPs- Diosgenin encapsulated Poly (D, L-lactic-co-glycolic) acid nanoparticles PBS- Phosphate buffered saline ABS- Acetate buffered saline EE-Entrapment efficiency LC-Loading capacity ROS-Reactive oxygen species GSH-Reduced glutathione GSSG-Oxidized glutathione LDH-Lactate dehydrogenase

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Section A-Research paper

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